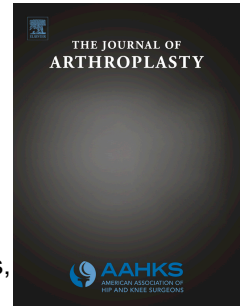


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Development and Verification of Novel Porous Titanium Metaphyseal Cones for Revision Total Knee Arthroplasty

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1 **Development and Verification of Novel Porous Titanium Metaphyseal Cones for**
2 **Revision Total Knee Arthroplasty**

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1 **Development and Verification of Novel Porous Titanium Metaphyseal Cones for**
2 **Revision Total Knee Arthroplasty**

3 **Abstract**

4 **Background:** Porous metaphyseal cones are widely used in revision knee arthroplasty. A
5 new system of porous titanium metaphyseal cones has been designed based on the
6 femoral and tibial morphology derived from a CT based anatomical database. The
7 purpose of this study is to evaluate the initial mechanical stability of the new porous
8 titanium revision cone system by measuring the micromotion under physiologic loading
9 compared to a widely-used existing porous tantalum metaphyseal cone system.

10 **Methods:** The new cones were designed to precisely fit the femoral and tibial anatomy,
11 and 3D printing technology was used to manufacture these porous titanium cones. The
12 stability of the new titanium cones and the widely used tantalum cones were compared
13 under physiologic loading conditions in bench top test model.

14 **Results:** The stability of the new titanium cones was either equivalent or better than the
15 tantalum cones. The new titanium femoral cone construct had significantly less
16 micromotion compared to the traditional femoral cone construct in 5 of the 12 directions
17 measured ($p < 0.05$) while no statistical difference was found in 7 directions. The new
18 porous titanium metaphyseal tibial cones demonstrated less micromotion in medial
19 varus/valgus ($p = 0.004$) and posterior compressive micromotion ($p = 0.002$) compared to
20 the traditional porous tantalum system.

21 **Conclusion:** The findings of this biomechanical study demonstrate satisfactory
22 mechanical stability of an anatomical-based porous titanium metaphyseal cone system for
23 femoral and tibial bone loss as measured by micromotion under physiologic loading. The

24 new cone design, in combination with instrumentation that facilitates surgical efficiency,

25 is encouraging. Long term clinical follow up is warranted.

26 **Keywords:** Knee revision cones, 3D printing, porous titanium, micromotion

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28 **Background**

29 Revision total knee arthroplasty (TKA) is a growing procedure with varying case
30 complexity. It is estimated that the number of revision TKAs performed in the United
31 States is projected to grow from 38,000 in 2005 to 268,200 by the year 2030 placing a
32 large burden on health care costs [1, 2]. Complex revision cases often present with
33 significant metaphyseal bone loss, which may be due to infection, osteolysis, loosening
34 of the primary implant or iatrogenic loss with implant resection. Larger bone defects
35 require more extensive reconstructive efforts and have been traditionally managed with
36 the use of large structural allografts [3-12], impaction bone grafting techniques with or
37 without mesh augmentation [13-16], fabrication of custom prosthetic components [17], or
38 the use of specialized hinged knee components [18]. In the past decade, large
39 metaphyseal defects have been effectively managed with partially porous metal stepped
40 “sleeves” or porous tantalum metaphyseal cones, both of which have excellent early term
41 results [19-27]. Addressing the bone loss can be challenging and the optimal
42 reconstruction method is often debated and remains unknown.

43 While porous metaphyseal cones have shown high success rates in the short and
44 mid-term [19, 22, 23, 25, 26], the existing cones have demonstrated some limitations
45 regarding geometry and size in comparison to the bony anatomy and defects encountered
46 in revision knee arthroplasty. This creates an intraoperative challenge for the surgeon to
47 reproducibly and accurately contour the bone to accurately match the implant chosen.
48 The process of machining the bone accurately may be technically challenging.

49 A new system of porous titanium metaphyseal cones have been designed based on
50 the femoral and tibial morphology derived from a CT based anatomical database. The

51 purpose of this study is to evaluate the initial mechanical stability of the new porous
52 titanium revision cone system by measuring the micromotion under physiologic loading
53 compared to a widely-used existing porous tantalum metaphyseal cone system.

54 **Materials and Methods**

55 The new porous titanium metaphyseal cone implants were designed to be used
56 with an accompanying instrumentation system to accurately and precisely fit the anatomy
57 of the proximal tibia and distal femur. These revision cone geometries are manufactured
58 from porous titanium (Tritanium, Stryker, Mahwah, NJ) using state of the art additive
59 manufacturing techniques. The anatomy-based fit was achieved by using an extensive
60 database of CT scans (SOMA, Stryker, Mahwah, NJ), which creates 3D models of the
61 proximal tibia and distal femur and delineates the cortical boundaries of the bone. A
62 more detailed description of SOMA and its application in implant design can be found
63 elsewhere [28-31]. A virtual revision TKA algorithm was established on 478 tibias (mean
64 age 58 and 40% male) and 921 femurs (mean age 58 and 56% male). The virtual
65 intramedullary (IM) canal was identified and used to determine alignment and the bone
66 resection plane. Revision resections of 13mm on the tibia and 11mm on the femur were
67 performed to approximate additional bone loss inherent with implant removal during a
68 revision procedure. Tibial baseplate sizing was determined based on rotation oriented to
69 the medial third of the tubercle and tibial plateau coverage with less than 1mm of
70 overhang. Femoral component rotation and sizing was based on approximating the
71 posterior condyles to restore the posterior condylar offset and anterior cortical run-out to
72 avoid notching and maximize anterior cortical contact. The femoral component rotation
73 was aligned with the epicondylar axis.

74 A series of conical cuts were modeled in SOMA representing the shape of
75 metaphyseal cones in three distinct geometries, (Figure 1). Figure 2 illustrates these
76 geometries assembled to bone models with compatible revision knee components.
77 Measurements were taken from the simulated reamer axes to the outer shell of the
78 cortical bone to characterize acceptable cone size, as illustrated in Figures 3.
79 Appropriate sizing and “fit” was identified by the scenario that maximized host bone
80 contact but within the cortical boundaries of the CT scan model for a given implant. Final
81 cone designs are illustrated in Figure 4.

82 *Femoral micromotion*

83 Seventeen composite femurs (Sawbones; Pacific Research, Vashon, WA) with a
84 cancellous analog of 20 pound per cubic foot (pcf) density were used for this study. The
85 composite femurs were prepared according to the surgical protocols of the new porous
86 titanium design (Triathlon Tritanium Cone Augments System, Stryker, Mahwah, NJ) and
87 the traditional porous tantalum design (Trabecular Metal Revision Knee System, Zimmer,
88 Warsaw, IN). An experienced revision arthroplasty surgeon was enlisted to prepare the
89 composite femurs for the traditional porous tantalum cone system in order to more
90 accurately simulate the in vivo technique and preparation with a high-speed burr. The
91 new porous titanium cones were prepared with a reamer-based system designed to
92 provide an intimate fit with the bone per the surgical protocol. A series of conical
93 reamers prepared the central base with adjacent medial and lateral “lobed” portions via
94 controlled and guided instrumentation, Figure 5. Ten of the new porous titanium cones
95 and seven of the traditional porous tantalum cones were implanted. Medium size femoral
96 components from both systems were used for this test. The new cone system utilized a

97 50mm stem. Since the traditional system has a taller boss, a 30mm stem was used. The
98 total boss/stem length for both systems was 75mm.

99 The cemented femur/cones constructs were spray painted with a black and white
100 speckle pattern on the lateral side as per protocol for the optical micromotion
101 measurements and then mounted to a six-station knee joint wear simulator. A line of sight
102 optical measurement system was used to track the speckle pattern to measure
103 micromotion between the implant construct and femur. Loading which replicated a level
104 walking activity was simulated for 154,000 cycles. The cycle count represents the
105 number of walking steps taken during the time for biological fixation to occur, typically a
106 6-week time period [32, 33]. Micromotion was measured in the x, y, and z directions at
107 the midpoints of the anterior flange, anterior chamfer, posterior chamfer and posterior
108 condyles between the composite femurs and the femoral components, (Figure 6).

109 *Tibial micromotion*

110 Mechanical testing of the new porous titanium tibial cone system (Triathlon
111 Tritanium Cone Augments System, Stryker, Mahwah, NJ) and traditional porous
112 tantalum cones (Trabecular Metal Revision Knee System, Zimmer, Warsaw, IN) was
113 performed using linear variable displacement transducers (LVDT). Similar to the
114 femoral specimens, tibial composite specimens were prepared by an experienced revision
115 arthroplasty surgeon with the manufacturer-recommended surgical technique. The
116 traditional porous tantalum cones were prepared with a high-speed burr to shape the
117 proximal tibial in the approximate geometry to accept the implant in order to maximize
118 composite bone contact. Similarly the new porous titanium tibial cones were prepared
119 with a reamer-based system designed to provide a more intimate fit with the bone per the

120 surgical protocol. A central conical reamer was utilized to a particular depth and a
121 medial lobed shape prepared with a smaller conical reamer via controlled and guided
122 instrumentation, (Figure 7). Micromotion of the cemented baseplate/cone construct with
123 respect to the tibia was measured in 10 test models during a stair descent loading profile
124 (Figure 8) for 10,000 cycles. The number of cycles represents 6-8 weeks of stair descent
125 activity, again the approximate length of time for initiation of bone ingrowth to occur
126 according to published literature [32, 33]. Six LVDTs were placed on anterior, posterior,
127 medial and lateral aspects of the construct to measure varus/valgus displacement,
128 internal/external rotation, compression and lift off. The test setup is shown in Figure 9.

129 *Statistical Analysis*

130 Unpaired T-tests and one-sided T-tests were used to evaluate statistical comparison of
131 peak-to-peak micromotion, compression, and lift off between groups.

132 **Results**

133 *Computer simulation using CT Database (SOMA)*

134 The three types of cone designs shown in Figure 1 were evaluated in the CT scans
135 available in the SOMA database. The fit results of these cone designs under various
136 resection scenarios are presented in Tables 1 through 3. When the femoral cone
137 geometry was paired with its optimal femoral component size, the average fit was seen to
138 be 92% at the resection level and 60% when buried 5mm deeper into the bone (Table 3).

139 The analysis demonstrated that the symmetric porous titanium tibial cone
140 geometry fit an average of 98% at the identified original resection level and 96% at the
141 additional 5mm resection level (5mm more distal on the tibia) of all bones when used
142 with the optimally compatible tibial baseplate (Table 1). When analyzing the fit of the

143 asymmetric tibial cone geometry, up to 10° of rotation around the tibial axis
144 (internal/external rotation) with respect to the tibial baseplate was allowed. This
145 rotational freedom is desirable in a surgical application where bone void size and location
146 is not totally aligned with the optimal tibial component rotation approximately at the
147 level of the medial one-third of tibial tubercle width. At neutral rotation to the tibial
148 implant, the asymmetric tibial cone geometry fit an average of 87% of bones at the
149 resection level and 38% of bones when 5mm below the original resection level. When
150 10° of internal rotation was utilized, the asymmetric tibial cone fit increased to 97% of
151 bones at the resection level and 78% of bones when 5mm sub-flush (Table 2).

152 *Femoral Micromotion*

153 The micromotion results for the new porous titanium and traditional porous
154 tantalum femoral cone designs are presented in Table 4. The new titanium femoral cone
155 construct had significantly less micromotion compared to the traditional femoral cone
156 construct in 5 of the 12 directions measured ($p < 0.05$, Table 4). These results were noted
157 at the posterior condyle, anterior flange and anterior chamfer locations. Results in other
158 directions of motion were comparable between devices (Table 4).

159 *Tibial Micromotion*

160 The tibial micromotion test results are presented in Table 5. The new porous
161 titanium tibial metaphyseal cone system demonstrated similar micromotion values under
162 loading compared to traditional porous tantalum cone system with the numbers available
163 ($p \geq 0.05$) in internal external rotation, varus/valgus and lift off during a simulated stair
164 descent activity. The new porous titanium metaphyseal tibial cones demonstrated less

165 micromotion in medial varus/valgus ($p=0.004$) and posterior compressive micromotion
166 ($p=0.002$) compared to the traditional porous tantalum system.

167 **Discussion**

168 Porous metaphyseal cones and sleeves have emerged as a useful method to
169 accomplish the goal of providing structural support for tibial and femoral implants as
170 well as filling larger bone voids in revision TKA [19-27]. Short and medium term
171 evidence on tantalum cones now exists that supports the use of these implants in the
172 reconstruction of large tibial defects in revision TKA [19, 21-26]. Despite these clinical
173 results, the surgical preparation for these devices remains technically challenging. This
174 prompted the innovation of a new porous titanium metaphyseal cone system with an
175 anatomically based shape from three-dimensional modeling of an extensive CT database.
176 The main objective of the accompanying instrumentation was to facilitate efficient bone
177 preparation with an intimate press-fit and cortical contact for maximal stability. Implant
178 mechanical stability is essential for these cementless devices to successfully
179 osseointegrate and reconstitute the femoral or tibial metaphysis providing mechanical
180 support for the implant and associated cement mantle. The assumption in this study that
181 the traditional porous tantalum metaphyseal cones are an appropriate comparison for
182 what constitutes adequate mechanical stability is supported by the successful clinical
183 results of these devices. Early outcomes with highly porous metaphyseal tantalum cones
184 utilized in large tibial defects for revision total knee arthroplasty have been reported by
185 multiple authors [25, 26]. Meneghini et al reported a series of fifteen revision knee
186 arthroplasties that were performed with a porous tantalum metaphyseal tibial cone and
187 were followed for a minimum of two years. All tibial cones were found to be

188 osseointegrated radiographically and clinically at final follow up with no reported failures
189 [25]. In a series of sixteen revision total knee arthroplasties with severe tibial defects,
190 Long and Scuderi reported good results with osseointegration of the porous tantalum
191 cone 14/16 cases at a minimum 2-year follow up [26]. Similar results have been reported
192 in the femoral version of the porous tantalum metaphyseal cones [21-23]. Howard et al.
193 reported on twenty-four femoral porous tantalum cones in complex revision total knee
194 arthroplasty and found no radiographic failure or loosening at a minimum two years
195 follow up [23].

196 Longer-term results are also available with highly porous tantalum metaphyseal
197 tibial cones, and have demonstrated continued good results [19]. Kamath et al. recently
198 reported on 66 highly porous tibial metaphyseal cones used in Type 2 and 3 AORI tibial
199 defects. At a minimum 5-year follow-up, the authors report one revision for aseptic
200 loosening and one radiograph with progressive radiolucencies concerning for fibrous
201 ingrowth with a greater than 95% revision-free survivorship at latest follow up[19].

202 The results of this study demonstrate the relative equivalency, and in some
203 specific locations superiority, of the new porous titanium cones to the clinically
204 successful traditional porous tantalum cones with respect to mechanical stability as
205 measured by micromotion under physiologic loading. By virtue of the successful clinical
206 results of the porous tantalum cones in multiple series, and similarities between the
207 porous structure of porous tantalum and titanium, the porous titanium cones are expected
208 to perform well in theory. This methodology of demonstrating mechanical stability of an
209 innovative design compared to a successful predicate is accepted in the peer-reviewed
210 literature [34-37].

211 In addition to the top priority of clinical success, surgical efficiency is a very
212 important consideration for patients, surgeons and the healthcare system. With the ever
213 growing burden of revision knee arthroplasty and the projections of increasing demand
214 for these procedures, it is essential that arthroplasty surgeons maximize their surgical
215 efficiency in these lengthy and complex procedures. These new porous titanium
216 metaphyseal cones were designed to maximize surgical efficiency in several ways,
217 including through a geometric implant fit derived from an anatomical CT database and a
218 streamlined reamer-based instrumentation that eliminates non-instrumented manual high-
219 speed burring.

220 Our study does have limitations. First, the mechanical testing performed in this
221 study was performed on sawbones composite replicate femoral and tibial specimens,
222 which may not accurately represent the in vivo scenario of revision bone. However, we
223 believe the mechanical stability of devices is appropriately compared in these specimens
224 due to their homogeneity, which minimizes confounding variables associated with
225 cadaveric specimens. Further, this testing methodology has been accepted in the hip and
226 knee arthroplasty peer-reviewed literature [34-37]. Second, although the biologic
227 fixation potential of highly porous titanium has been studied and supported [38],
228 equivalency in osseointegration and subsequent interfacial strength of porous titanium
229 compared to the clinically successful porous tantalum has not been fully elucidated. This
230 underscores the need for close clinical follow up of these devices in the short and long
231 term in order to corroborate these biomechanical findings.

232 In summary, the findings of this biomechanical study demonstrate satisfactory
233 mechanical stability of an anatomical-based porous titanium metaphyseal cone system for

234 femoral and tibial bone loss as measured by micromotion under physiologic loading.
235 The findings of optimized mechanical stability of these new titanium cones compared to
236 the clinically successful porous tantalum cones, in combination with instrumentation that
237 facilitates surgical efficiency, is encouraging. However, close clinical follow up is
238 warranted and should include radiographic and clinical outcomes in the early and longer
239 term.
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Figure Legends

Fig 1: Modeling of three distinct conical geometries

Fig 2: Cone geometries assembled to bone models

Fig 3: Illustrates of measurements from simulated reamer axes to cortical bone that was used to determine cone fit

Fig 4: Illustration of the design of the symmetric, asymmetric and the femoral cones manufactured by additive manufacturing using porous titanium

Fig 5: Illustration of femoral preparation using central and medial/lateral lobe reamers

Fig 6: Micromotion measurement locations and direction

Fig 7: Illustration of tibial preparation using central and medial/lateral lobe reamers

Fig 8: Loading profile used in the study

Fig 9: Test set up for tibial micromotion test

Table 1: Simulated average fit results of the symmetric tibial cones for various orientations

Orientation	Average percentage of fit
Resection level, neutral rotation	98%
5mm below resection, neutral rotation	96%

Table 2: Simulated average fit results of the asymmetric tibial cones for various orientations

Orientation		Average percentage of fit
Resection level	Neutral rotation	87%
	10° Internal rotation	97%
5 mm below resection	Neutral rotation	38%
	10° Internal rotation	78%

Table 3: Simulated average fit results of the femoral cones for various orientations

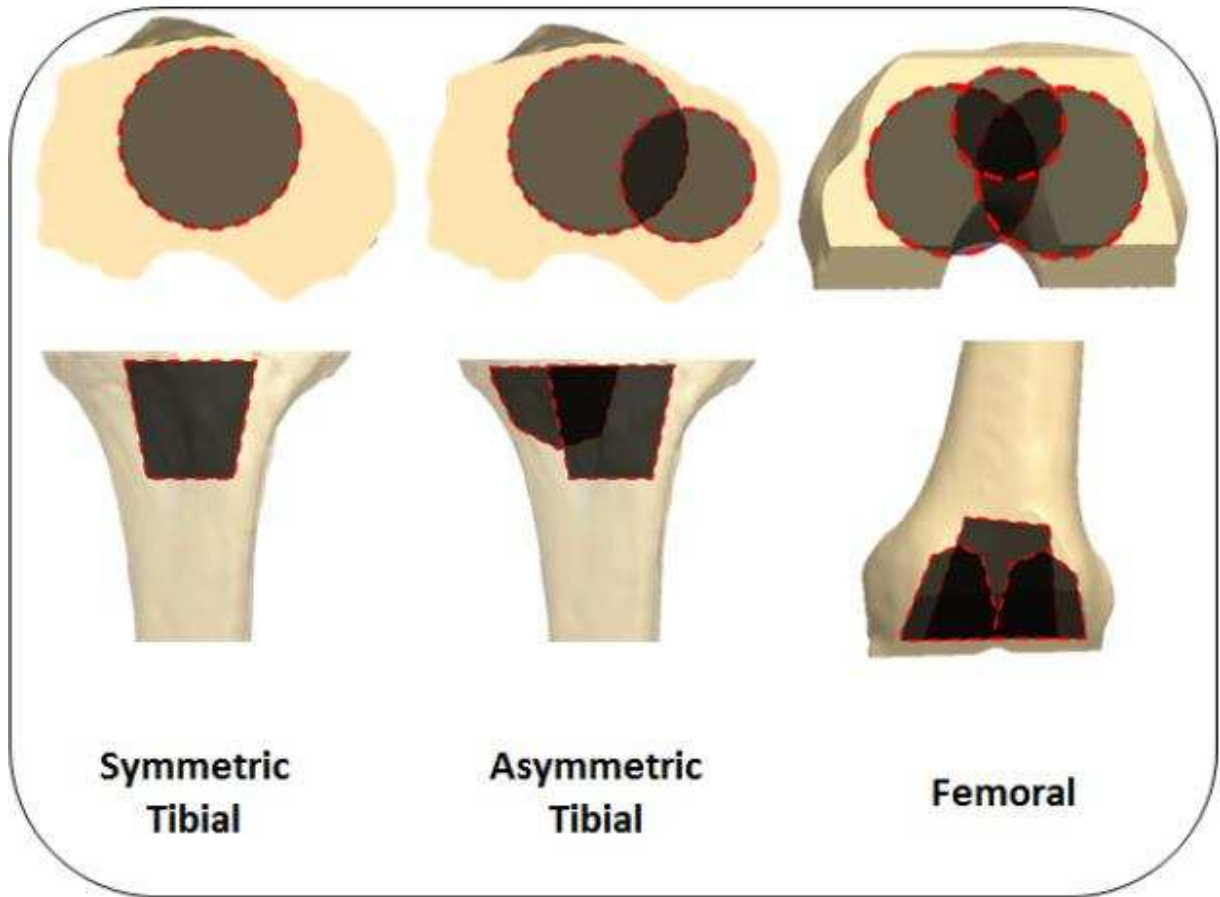
Orientation	Average percentage of fit
Resection level, neutral rotation	92%
5mm below resection, neutral rotation	60%

Table 4: Femoral micromotion results for the two cone systems. Bolded values indicate significant difference between New and Traditional Systems ($p < 0.05$).

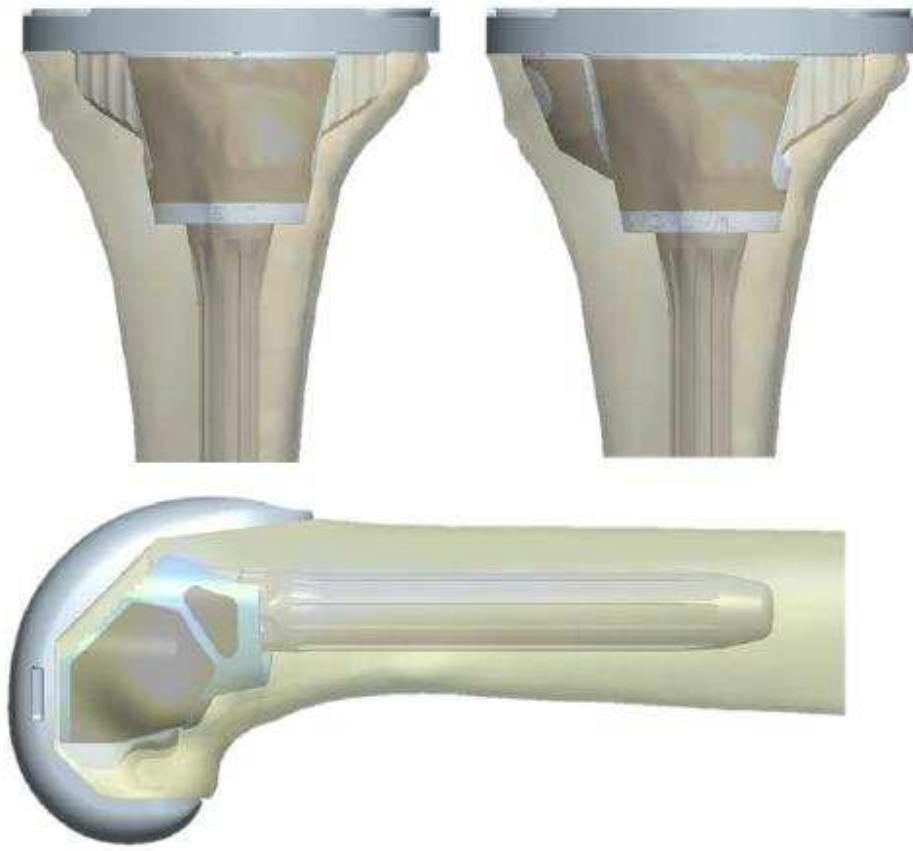
Design		Posterior condyle			Anterior flange			Anterior Chamfer			Posterior Chamfer		
		x	y	z	x	y	z	x	y	z	x	y	z
New cone system	Average	12.31	11.95	34.1	14.4	14.38	24.79	13.1	16.6	34.8	13.6	13.57	27.2
	SD	5.57	6.51	18.6	10.3	3.97	4.96	7.24	6.05	9.24	4.58	4.58	9.53
	N	10	10	10	10	10	10	10	10	10	10	10	10
Traditional cone system	Average	24.9	14.89	35.92	33.4	20.3	26.4	32.2	27.4	27.6	31.3	31.3	28.95
	SD	6.24	3.4	14.7	17.7	14.7	11.9	13.3	15.3	10.4	22.2	8.64	5.38
	N	7	7	7	7	7	7	7	7	7	7	7	7
t- test	p- value	0.001	0.122	0.388	0.007	0.169	0.374	0.004	0.61	0.917	0.04	0.039	0.319

Table 5: Tibial micromotion results for the two cone systems. Bolded values indicate significant difference between New and Traditional Systems ($p < 0.05$).

Design		Varus/Valgus motion		Internal/external rotation		Compression and lift off	
		Medial S/I (mm)	Lateral S/I (mm)	Medial A/P (mm)	Lateral A/P (mm)	Posterior S/I (mm)	Anterior S/I (mm)
New cone system	Average	0.029	0.05	0.021	0.011	0.036	0.013
	SD	0.012	0.009	0.008	0.012	0.007	0.003
	N	10	10	10	10	10	10
Traditional cone system	Average	0.064	0.055	0.023	0.008	0.069	0.033
	SD	0.025	0.009	0.005	0.003	0.02	0.029
	N	10	10	10	10	10	10
t- test	p- value	0.004	0.105	0.247	0.363	0.002	0.064

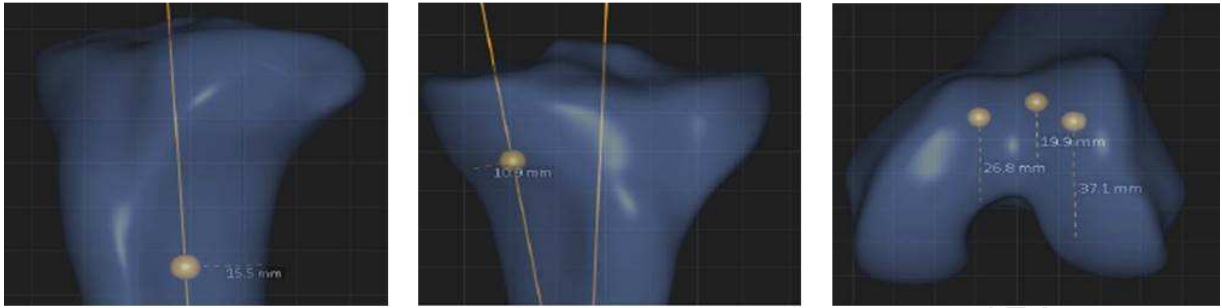


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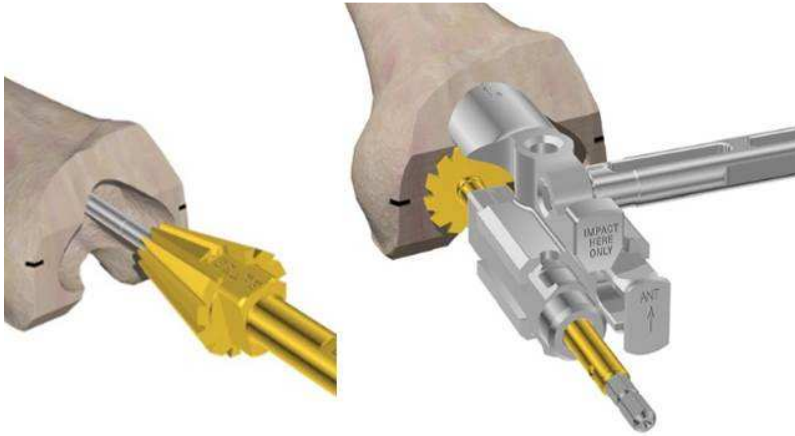
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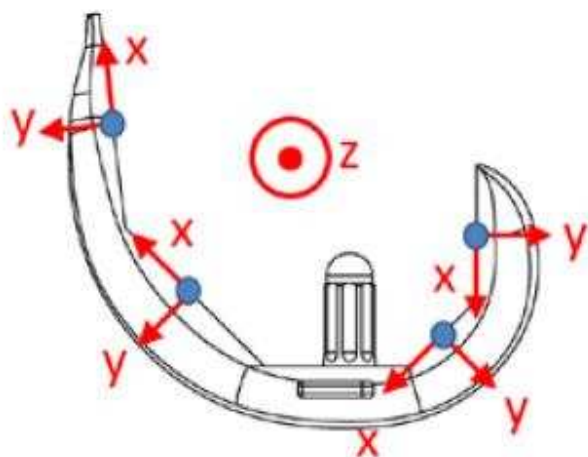
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